

The General Requirements for Biostudies

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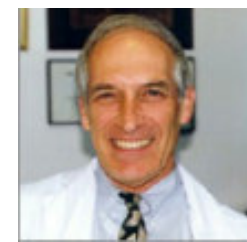
To bear in Remembrance...

Whenever a theory appears to you as the only possible one, take this as a sign that you have neither understood the theory nor the problem which it was intended to solve.



Karl R. Popper

Even though it's *applied* science we're dealin' with, it still is – *science!*



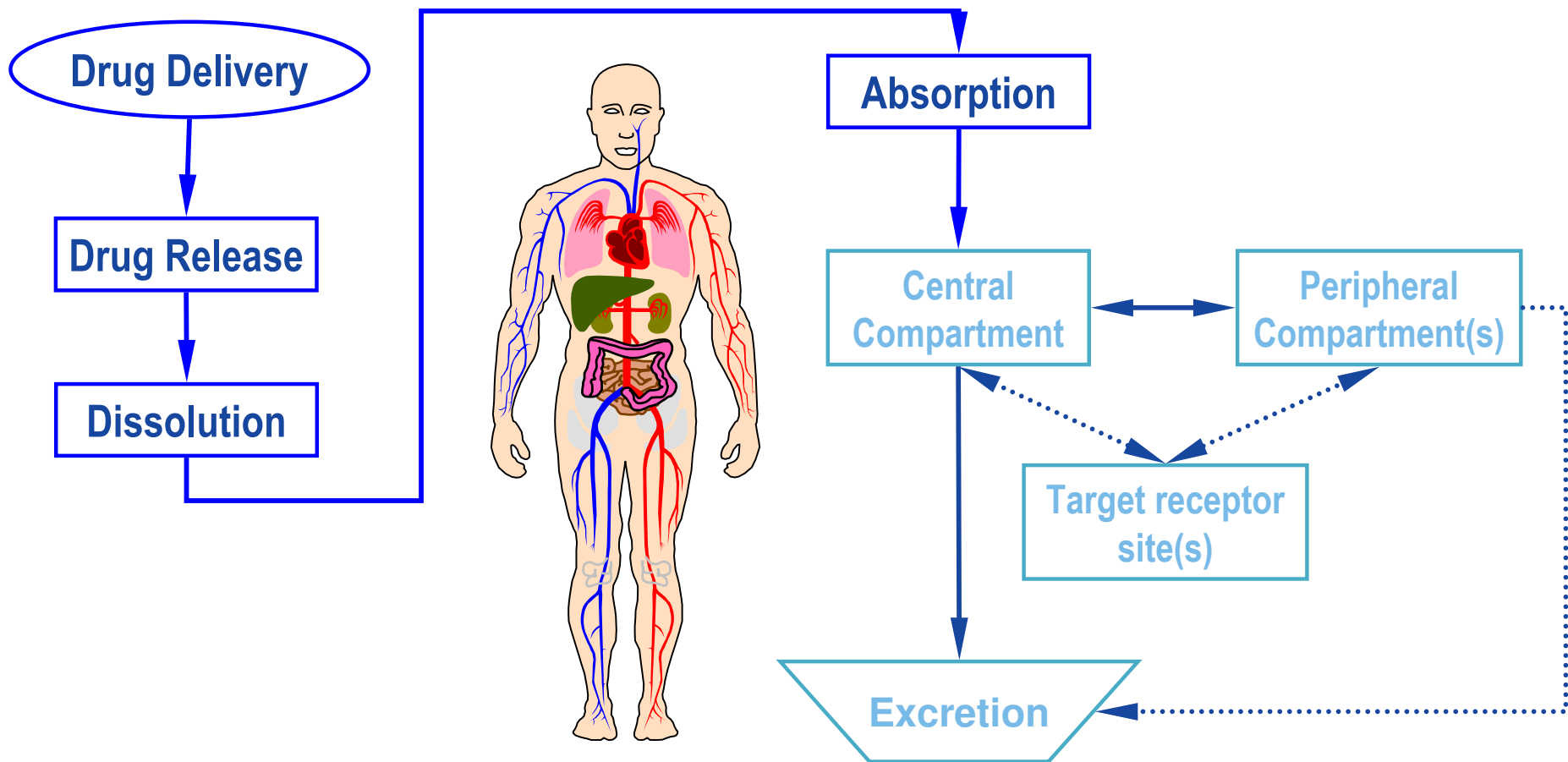
Leslie Z. Benet

Fundamentals of Pharmacokinetics

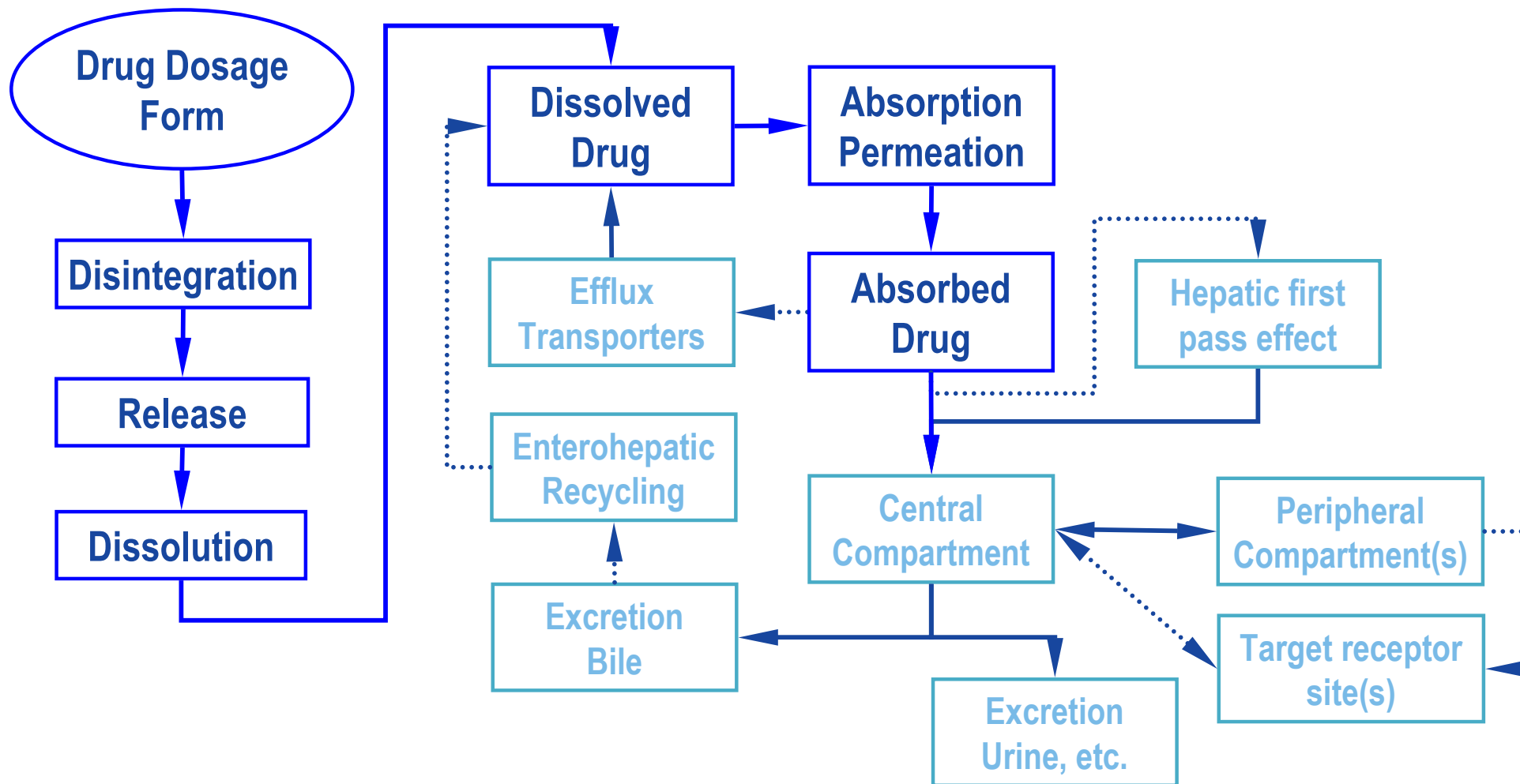
φαρμακός (drug) + κινητικός (putting in motion)

- Term introduced in 1953.
 - Friedrich H Dost 1953
Der Blutspiegel: Kinetik der Konzentrationsabläufe in der Kreislaufflüssigkeit
- *Pharmacokinetics* may be simply defined as what the body does to the drug, as opposed to *pharmacodynamics* which may be defined as what the drug does to the body.
 - Leslie Z. Benet 1984
Pharmacokinetics: Basic Principles and Its Use as a Tool in Drug Metabolism

Pharmacokinetic process



Pharmacokinetic process



Pharmacokinetic process

(L)ADME

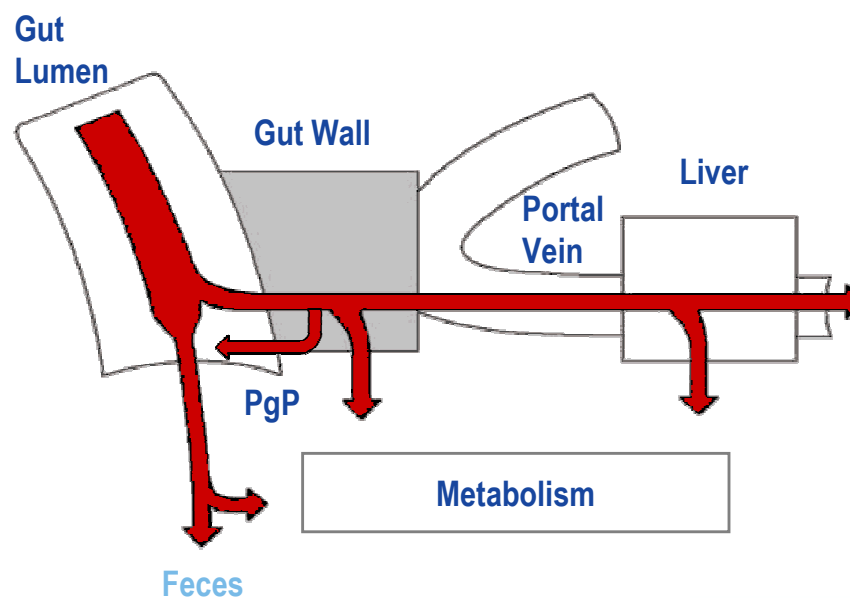
Biopharmaceutical phase

Disintegration
Release
Dissolution

} Liberation

Pharmacokinetic phase

Absorption
Passive diffusion
Active transport
Distribution
Metabolism
Intestinal first pass
Membrane first pass
Hepatic first pass
Excretion

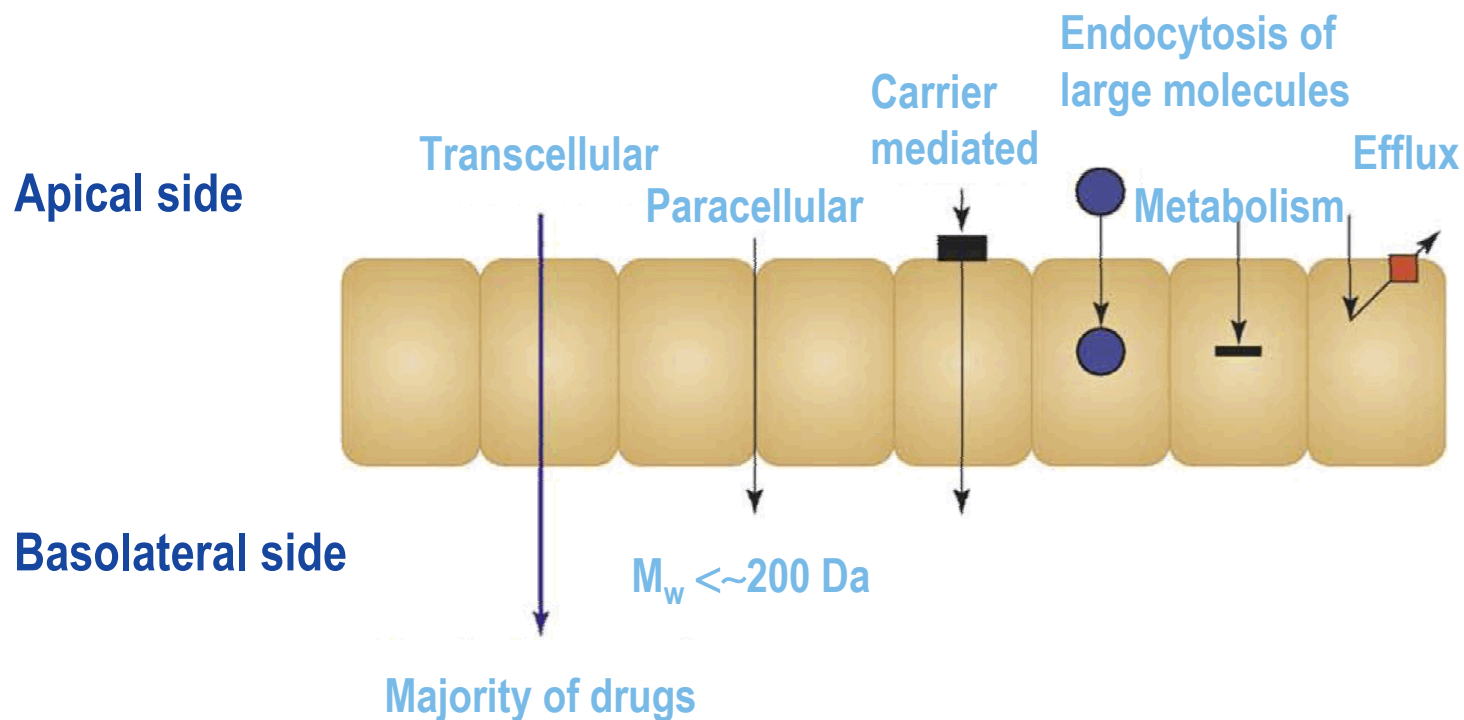


Central Compartment

Elimination = M + E

Pharmacokinetic process

Absorption revisited



Pharmacokinetic models

The body is simplified to one – or more –
'Compartments' where the drug is distributed

- One compartment model
 - Drug is distributed homogeneously within the entire body.
- Two compartment model
 - The first (central) compartment is *loosely* related to the blood and heavily perfused organs: Liver, kidneys, lung, muscles, (brain).
 - The second (peripheral) compartment describes less perfused tissues (fat, bones, ...).

Pharmacokinetic models

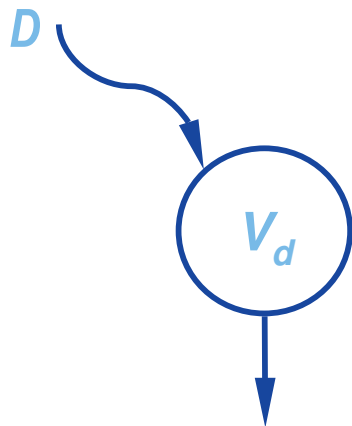
Compartment models

- **Compartments are**
 - described by a volume and
 - pathways which link them.
- **These links may be**
 - unidirectional (absorption, excretion) or
 - bidirectional (central \leftrightarrow peripheral)
- **Most common models are ‘mammillary’, *i.e.*,**
 - absorption to the central compartment,
 - distribution to peripheral and back to the central compartment, and
 - elimination from the central compartment.

Pharmacokinetic models

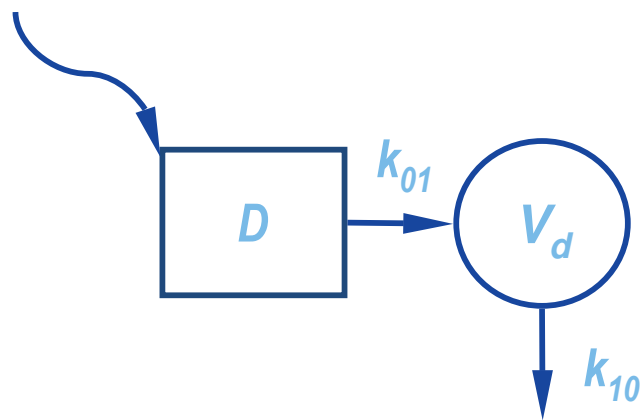
Examples

One comp. IV



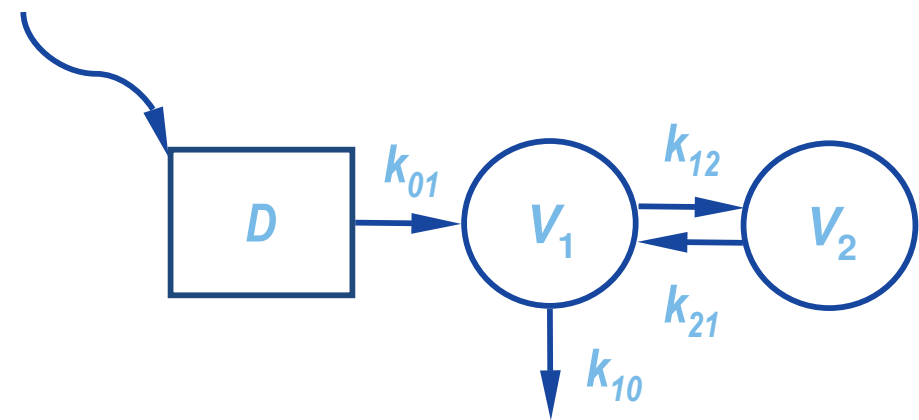
M + E

One comp. EV



A + M + E

Two comp's EV

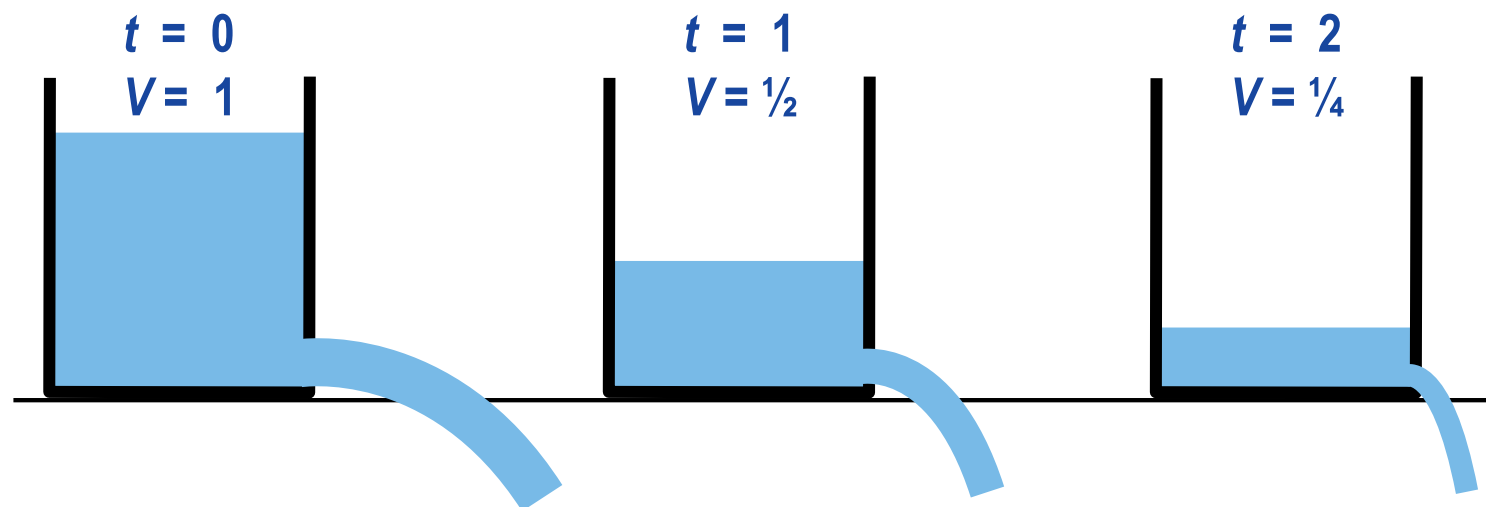


A + D + M + E

One compartment model, IV dose

Excursion into Hydrodynamics

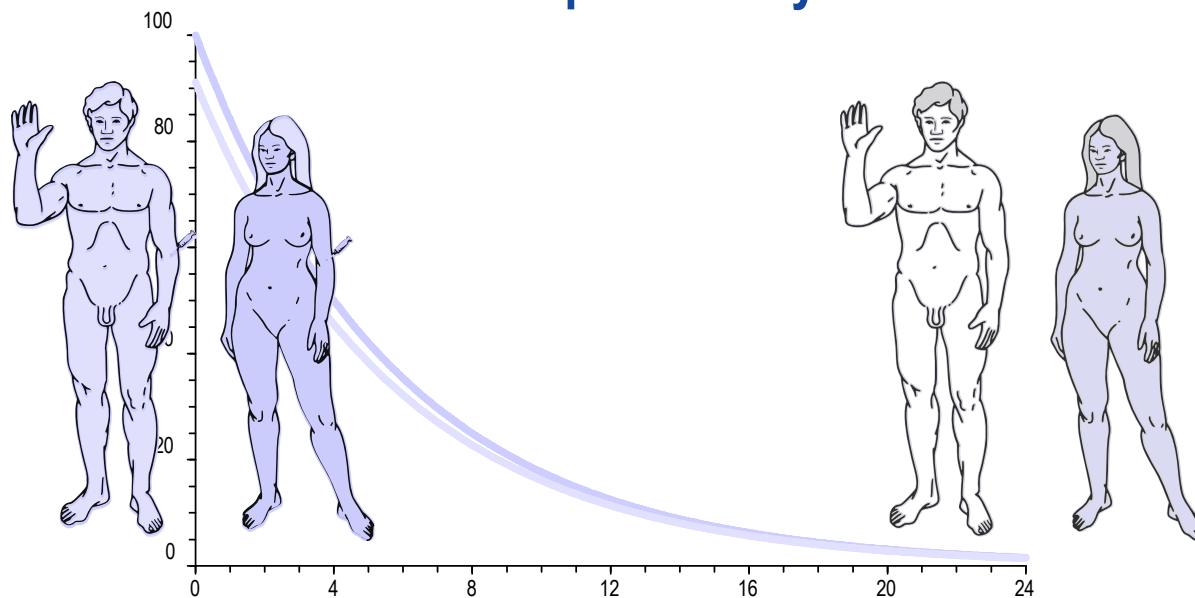
- Driving force for draining an *open* tank:
Hydrostatic pressure (height of liquid column & gravity).
- Emptied volume decreases with time.
- Same *proportion* is emptied in the same time interval.



One compartment model, IV dose

The whole body is simplified to one 'compartment'

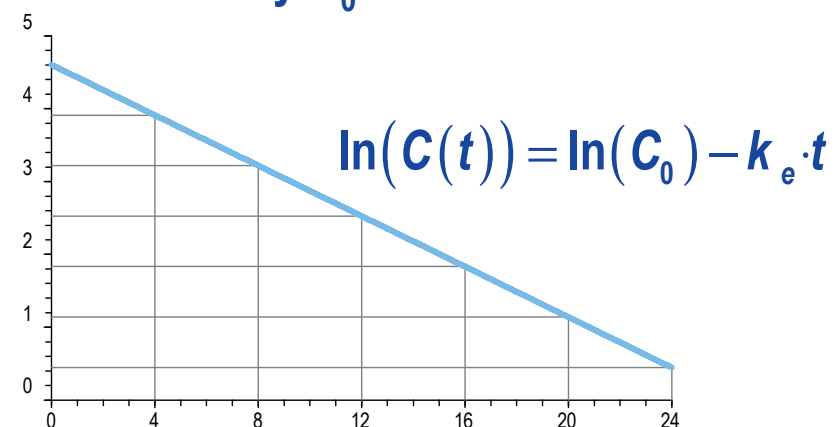
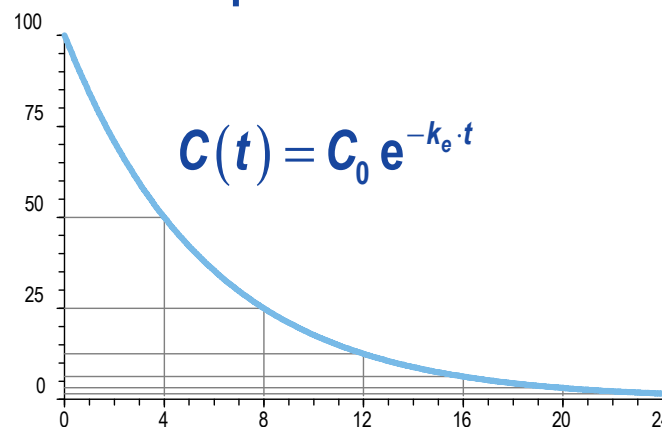
- Practically instantaneous distribution.
- Homogenous within all tissues.
- Concentrations decline exponentially.



One compartment model, IV dose

Half life

- Throughout the profile concentration drops to $\frac{1}{2}$ of its previous value within one 'half life' ($t_{1/2}$).
- In a semilogarithmic plot the profile shows a straight line with
 - a slope of $-\ln(2)/t_{1/2}$, which is the elimination rate constant k_e and
 - the intercept is related to the initial concentration by $C_0 = e^{\text{intercept}}$.



One compartment model, IV dose

Volume of distribution

- At administration the entire dose (D) is assumed to homogeneously dissolve in the 'Volume of distribution' (V_d).
- Only concentrations can be measured.
 - At $t = 0$ we get $V_d = \frac{C_0}{D}$.
 - **Cave:** V_d describes a *hypothetical* compartment, whereas in reality the distribution might not be homogenous. Some lipophilic drugs have a V_d of hundreds of liters...
 - Classical PK is *not* directly related to physiology.
 - Essentially, all models are wrong, but some are useful. *George Box*

One compartment model, IV dose

Clearance

- Instead of describing elimination by the rate constant k_e (unit: 1/time) we can also ask for the *fraction* of V_d which is completely ‘cleared’ of the drug per unit of time.
- This parameter is called ‘Clearance’ CL (unit: volume/time), which leads to basic equations of pharmacokinetics:

$$CL = V_d \cdot k_e \text{ or } \frac{D}{AUC}, \text{ where } AUC = \int_{t=0}^{t=\infty} C(t) dt$$

$$[\text{volume / time}] = \frac{[\text{mass}]}{[\text{time} \times \text{mass / volume}]}$$

Assumptions in Bioequivalence

All models rely on assumptions.

- Bioequivalence as a surrogate for therapeutic equivalence.
 - Studies in healthy volunteers in order to minimize variability (*i.e.*, lower sample sizes than in patients).
 - Current emphasis on *in vivo* release ('human dissolution apparatus').
- Concentrations in the sample matrix reflect concentrations at the target receptor site.
 - In the strict sense only valid in steady state.
 - *In vivo* similarity in healthy volunteers can be extrapolated to the patient population(s).
- $f = \mu_T / \mu_R$ assumes that
 - $D_T = D_R$ and
 - inter-occasion clearances are constant.

$$AUC_T = \frac{f_T \cdot D_T}{CL}, \quad AUC_R = \frac{f_R \cdot D_R}{CL}$$

Regulatory demands for study design in BE

Definitions

- EMA (BE-GL, 2010)
 - Two medicinal products containing the **same active substance** are considered **bioequivalent** if they are **pharmaceutically equivalent or pharmaceutical alternatives** and their **bioavailabilities** (rate and extent) after administration in the **same molar dose** lie within **acceptable predefined limits**. These limits are set to ensure comparable *in vivo* performance, *i.e.* similarity in terms of safety and efficacy.
- FDA (CFR 21–320.1, 2016)
 - **Bioequivalence** means the **absence of a significant difference in the rate and extent** to which the active ingredient or active moiety in **pharmaceutical equivalents or pharmaceutical alternatives** becomes available at the site of drug action when administered at the **same molar dose** under similar conditions in an appropriately designed study.

Regulatory demands for study design in BE

BE = (Desired) result of a comparative bioavailability study.

- **Generally only for extravascular routes. Exceptions for IV:**
 - Excipients which may interact with the API (complex formation).
 - Case-by-case: Liposomal formulations, emulsions.
- **Same active substance.**
 - Focus on the ‘core’ API (*different* salts, esters, isomers, complexes are considered the *same* active substance).
- **Same molar dose.**
- **Clinically not relevant difference: Δ 20% (NTIDs 10%, HVD(P)s >20%).**
- **100(1 – 2 α) confidence interval of PK-metrics within $[1 - \Delta, (1 - \Delta)^{-1}]$.**
 - AUC_{0-t} (extent of absorption)
 - C_{max} (rate of absorption)
 - t_{max} , AUC_{0-T} , $C_{max,ss}$, $C_{min,ss}$, $C_{T,ss}$, %PTF, partial AUCs, ...

Regulatory demands for study design in BE

Design should allow accurate (unbiased) assessment of the treatment effect.

- **Generally healthy volunteers (lower variability); except:**
 - Not ethical due to effects or AEs → study in patients.
- **Cross-over design preferred.**
 - Each subject serves as its own 'reference'.
 - Hence, the comparison is performed *within* subjects.
 - More powerful (fewer subjects needed) than in a parallel design.
- **Parallel design as an alternative.**
 - Studies in patients where the disease state is not stable.
 - Studies of drugs with (very) long half lives.
 - Comparison is performed *between* subjects.
 - Less powerful than cross-over.
 - Requires high degree of standardization.

Regulatory demands for study design in BE

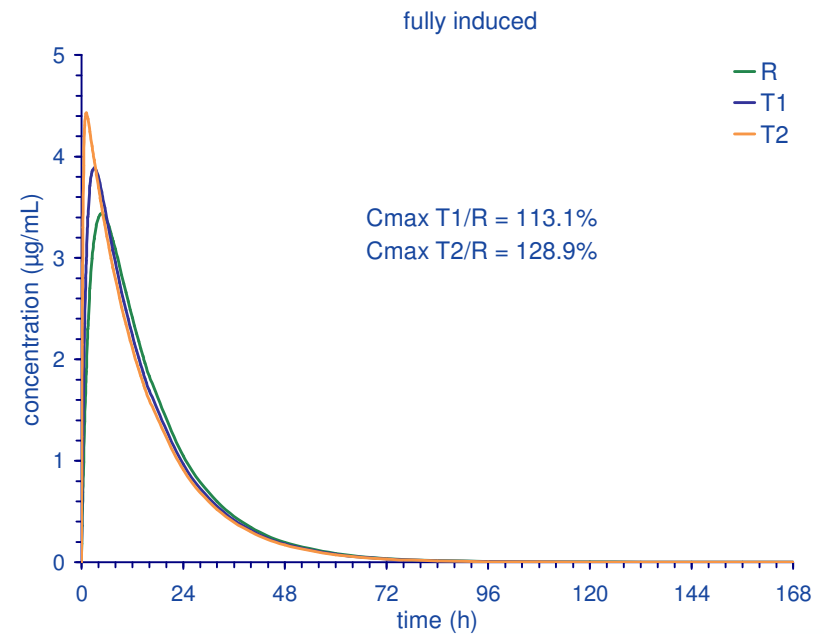
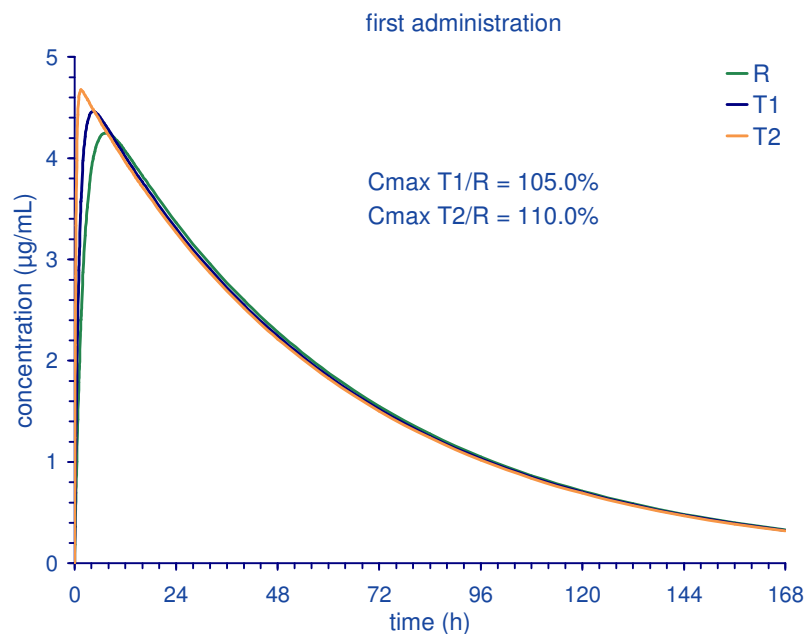
Design should allow accurate (unbiased) assessment of the treatment effect.

- **Cross-over design.**
 - Assumes that the treatment effect is independent from the period and sequence of administration.
 - Sufficiently long washout between periods:
 - » No residual concentrations in higher period(s).
 - » No remaining effect which may influence ADME.
 - » Patients: Stable disease.
- **Parallel design.**
 - Assumes lacking difference in groups.
 - Similar anthropometric properties (sex, age, BMI, ...).
 - If the drug is subjected to polymorphism, geno-/phenotyping is mandatory.

Regulatory demands for study design in BE

Design should allow accurate (unbiased) assessment of the treatment effect.

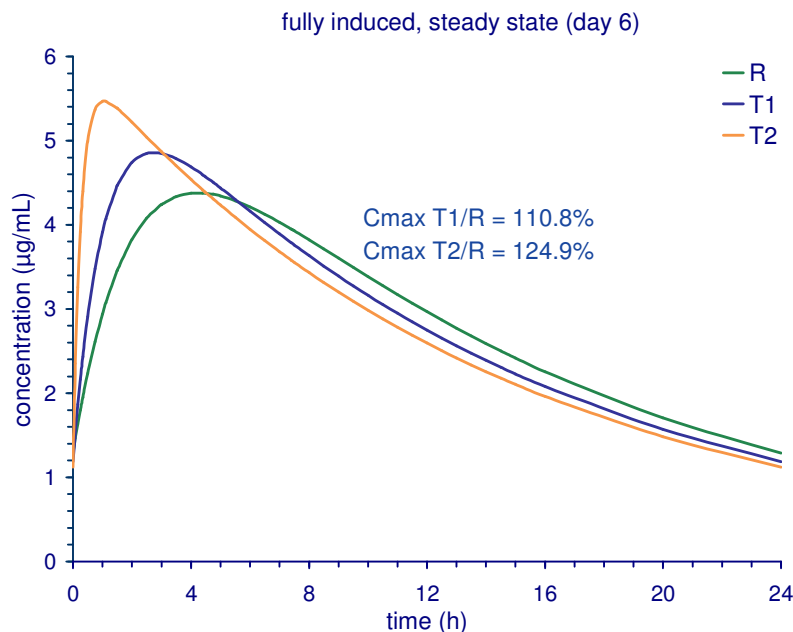
- What about auto-induction? Warfarin ($k_{a(R)}$ 0.472, $k_{a(T1)}$ 0.94, $k_{a(T2)}$ 3.6).
 - $t_{1/2}$ after first administration 43 hours.
 - Decreases to 10 hours after full induction.



Regulatory demands for study design in BE

Design should allow accurate (unbiased) assessment of the treatment effect.

- The NTID warfarin.
 - One of the rare examples where MD-studies (in steady state) are more sensitive to detect differences in the rate of absorption than SD-studies.



Regulatory demands for study design in BE

Design should be able to detect differences in formulations.

- Parent vs. metabolite(s).
 - Absorption of parent expected to be the best measure of Liberation and Absorption (formulation dependent).
 - Parent may be difficult to measure (pro-drugs: low concentrations together with fast elimination).
 - Alternative: metabolite (irrelevant whether active or inactive).
 - If possible measure the *first* metabolite in the chain. The further 'downstream' a metabolite is, the less it is able to detect differences in absorption of the parent.
- Fasting vs. fed.
 - Generally fasting since considered the most sensitive.
 - Exceptions:
 - » Intake *with* food required according to the reference's SmPC.
 - » Fasting *and* fed for MR products (EMA, some product-specific guidance by the FDA).

Regulatory demands for study design in BE

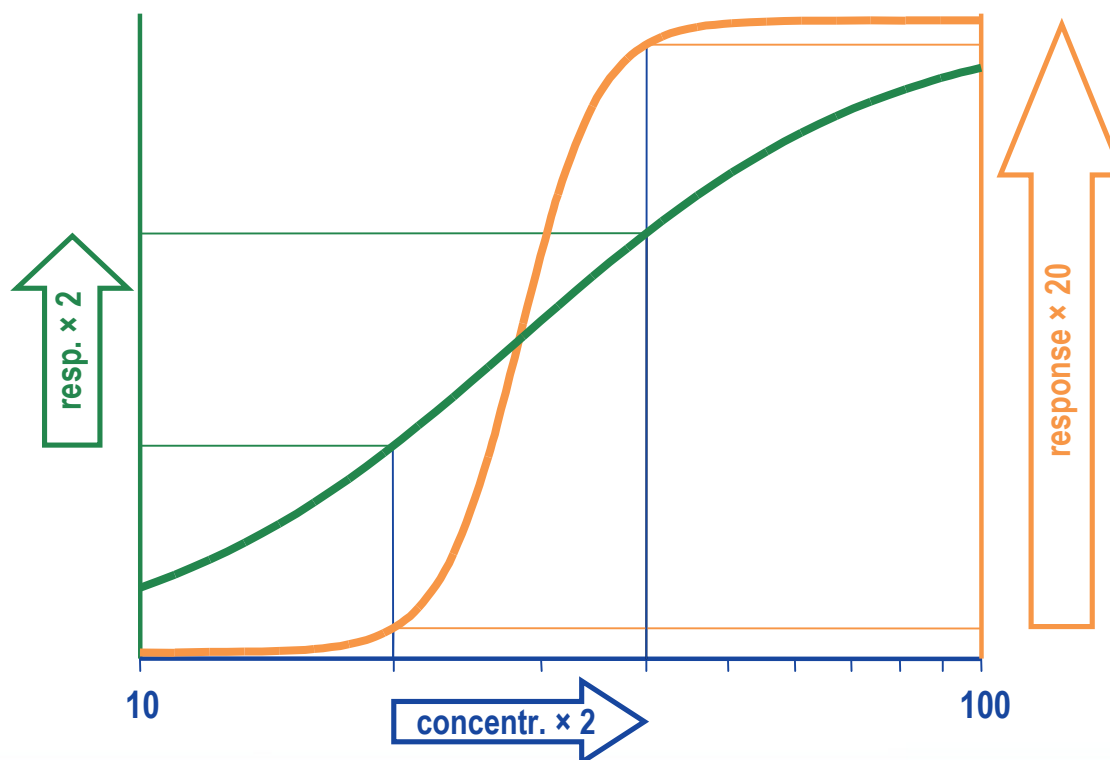
Design should be able to detect differences in formulations.

- **Dose strength.**
 - The strength which is considered to be most sensitive.
 - **Linear PK:**
 - Generally highest strength.
 - If highly soluble, a lower strength is acceptable.
 - A lower strength is also acceptable if safety/tolerability issues in healthy subjects (requires justification).
 - **Nonlinear PK:**
 - Higher than proportional increase in AUC over the dose range:
 - » Generally highest strength. Similar exceptions as for linear PK.
 - Lower than proportional increase in AUC over the dose range:
 - » *Lowest and highest strength.*
 - » Under certain conditions testing only the lowest strength can be justified.

Narrow therapeutic index drugs and HVDP(s)

Clinically not relevant difference.

- Based on PK but extrapolated to similarity of safety and efficacy in the patient population.
 - Depends on the dose-response curve! NTID (steep curve), HVD (flat curve):



Narrow therapeutic index drugs and HVDP(s)

Clinically not relevant difference.

- Based on PK but extrapolated to similarity of safety and efficacy in the patient population.
 - Predefined by the authority.
 - Generally 20%.
 - » Leads to BE-limits of 80.00–125.00%.
 - Lower for NTIDs.
 - » EMA: 10% leads to BE-limits of 90.00 – 111.11%.
 - » FDA: Scaled based on the variability of the reference.

CV_{WR}	BE-limits (%)
5.00	94.87 – 105.41
7.50	92.41 – 108.21
10.03	90.00 – 111.11
15.00	85.46 – 117.02
20.00	81.17 – 123.20
21.50	80.00 – 125.00

Narrow therapeutic index drugs and HVDP(s)

Clinically not relevant difference.

- Based on PK but extrapolated to similarity of safety and efficacy in the patient population.
 - Predefined by the authority.
 - Higher for HVD(P)s. Scaled based on the variability of the reference.
 - » EMA: IR C_{max} only; MR (additionally $C_{max,ss}$, $C_{min,ss}$, $C_{T,ss}$, partial AUCs).
 - » FDA: C_{max} , AUC.
 - » HC: AUC only.

EMA		FDA		HC	
CV_{WR}	BE limits (%)	CV_{WR}	BE limits (%)	CV_{WR}	BE limits (%)
≤ 30	80.00 – 125.00	≤ 30	80.00 – 125.00	≤ 30	80.00 – 125.00
35	77.23 – 129.48	35	73.83 – 135.45	35	77.23 – 129.48
40	74.62 – 143.02	40	70.90 – 141.04	40	74.62 – 143.02
45	72.15 – 138.59	45	68.16 – 146.71	45	72.15 – 138.59
≥ 50	69.84 – 143.19	50	65.60 – 152.45	50	69.84 – 143.19
		60	60.96 – 164.04	≥ 57.4	66.67 – 150.00

Plasma levels or alternatives

Recap the main assumption:

- Concentrations in the sample matrix reflect concentrations at the target receptor site.
 - In exceptional cases neither the parent or a metabolite can be reliably measured. Needs good justification – a simple claim is not sufficient!
 - Urine may be used as an alternative matrix, if
 - the drug shows high absolute bioavailability and
 - is mainly excreted unchanged in the urine.
 - With the current analytical technology of historical interest.
 - Example: Bisphosphonates (very low and highly variable absorption).
 - » *AUC* as the PK metric for extent of absorption could not be reliably measured in plasma.
The amount excreted in urine was employed instead.
 - » However, C_{max} in plasma was still required as the PK metric for the rate of absorption.

Plasma levels or alternatives

Recap the main assumption:

- Concentrations in the sample matrix reflect concentrations at the target receptor site.
 - Sometimes the receptor site is *not* directly linked to the circulation.
 - Example: Pulmonary delivery of antiasthmatics.
 - » Receptors are located in the lung.
 - » Drug acts *locally*.
 - » By inhalation the dose is fractionated:
 - (a) deposited in the lung (responsible for the effect) and subsequently absorbed (bypassing first-pass metabolism),
 - (b) absorbed in the oral cavity (bypassing first-pass metabolism),
 - (c) swallowed and absorbed in the GIT (subjected to metabolism).
 - » Only (a) reflects the effect.
 - » EMA: By administering charcoal we block (b) and (c). Now can measure the drug in plasma (absorbed through the lung only).
 - » FDA: Measurement of a *pharmacodynamic* surrogate (FEV₁).

The General Requirements for Biostudies

Thank You!
Open Questions?



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